

### IN THE SPECIFICATION

Please make the amendment indicated below in the paragraph that begins at page 8, line 9.

Although fluoropolymers have been among the most commonly used materials for blood-contacting devices, polyurethanes, polyethylene terephthalates ("PETs") and numerous other fluorinated and non-fluorinated polymers have also found considerable application. Modifications of polyurethanes, PETs and other plastics have included the introduction of coatings for antithrombogenic and anticoagulant properties. PET is an example of a non-fluorinated polymer that is highly hydrophobic and therefore difficult to coat with polar, aqueous materials such as heparin. PTFE is but one example of the general chemical class of fluoropolymer[[.]] that also includes FEP (fluorinated ethylene propylene), PFA (perfluoroalkyl vinyl ether and tetrafluoroethylene co-polymer), PVDF (polyvinylidenedifluoride), PVF (polyvinylfluoride), PCTFE (polychlorotrifluoroethylene), ETFE (ethylene and tetrafluoroethylene co-polymer) TFB (terpolymer of vinylidenedifluoride, hexafluoropropylene and tetrafluoroethylene) and other fluoropolymers as known in the art and described in many references including, for example, W. Woebcken in Saechtling International Plastics Handbook for the Technologist, Engineer and User, 3<sup>rd</sup> Ed., (Hanser Publishers, 1995) pp. 234-240, incorporated herein by reference.

Please replace the paragraph that begins at page 9, line 15 with the following replacement paragraph:

A hemocompatible coating is dissolved in a mixture of solvents in which a first solvent wets the polymer to be coated and the second solvent enhances the solubility of the hemocompatible coating material in the solvent mixture. First solvents that have the property of wetting hydrophobic polymers are typically nonpolar. Typical second solvents include polar solvents such as organic alcohols, ketones, among other possibilities. In one embodiment, azeotropic mixtures of the second solvent in the first solvent are used, although concentrations of the second solvent from near zero up to saturation may be used. The present invention also relates to medical devices, including endoluminal stents, that employ the coated materials of the present invention. Producing a porous material having a hemocompatible coating on at least some blood-

contacting surfaces thereof is a primary object of the present invention. Medical devices using such materials in a blood-contacting environment have the advantages of reducing the accumulation of platelets and thrombus on the coated surfaces.

Please replace the paragraph that begins on page 13, line 21 with the following replacement paragraph:

One example of a substantially azeotropic mixture described in detail below includes a polymer-wetting solvent HCFC-225 containing about 6% methanol (by volume). This solvent mixture is found to be adequate in[[ the]] some embodiments of the present invention. "HCFC-225" is a mixture of isomers of dichloropentafluoropropane, typically HCFC-225ca is  $\text{CF}_3\text{CF}_2\text{CHCl}_2$  and HCFC225cb is  $\text{CClF}_2\text{CF}_2\text{CHFCl}$ . However, azeotropic mixtures are not necessary in the present invention and adequate results are obtained with concentrations of polar solvent from approximately 0.00001% up to saturation of the polar solvent dissolved in the non-polar solvent. In some embodiments of the present invention, concentrations of polar solvent in the range from about 0.1% to about 10% by volume are used. However, while the above ranges give therapeutically useful amounts of hemocompatible coatings, better quality coatings are typically obtained with concentrations in the range from approximately 0.1% to approximately 2%. A range from approximately 0.5% to approximately 1% is particularly useful in that 0.5% has enough hemocompatible material for therapeutically effective coatings ~~by~~ but 1% is dilute enough to avoid webbing.